

1 **Optimizing A Therapeutic Humanized Follicle-Stimulating Hormone–Blocking Antibody**  
2 **Formulation By Protein Thermal Shift Assay**

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20 Short Title: Formulating FSH Blocking Antibody

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1 **ABSTRACT**

2 Biopharmaceutical products are formulated using several Food and Drug Administration  
3 (FDA) approved excipients within the inactive ingredient limit to maintain their storage stability  
4 and shelf life. Here, we have screened and optimized different sets of excipient combinations to  
5 yield a thermally stable formulation for the humanized follicle-stimulating hormone (FSH)–  
6 blocking antibody, MS-Hu6. We used a protein thermal shift assay in which rising temperatures  
7 resulted in the maximal unfolding of the protein at the melting temperature ( $T_m$ ). To determine  
8 the buffer and pH for a stable solution, four different buffers with a pH range from 3 to 8 were  
9 screened. This resulted in maximal  $T_m$ s at pH 5.62 for Fab in phosphate buffer and at pH 6.85  
10 for Fc in histidine buffer. Upon testing a range of salt concentrations, MS-Hu6 was found to be  
11 more stable at lower concentrations, likely due to reduced hydrophobic effects. Molecular  
12 dynamics simulations revealed a higher root-mean-square deviation with 1 mM than with 100 mM  
13 salt, indicating enhanced stability, as noted experimentally. Among the stabilizers tested, Tween  
14 20 was found to yield the highest  $T_m$  and reversed the salt effect. Among several polyols/sugars,  
15 trehalose and sucrose were found to produce higher thermal stabilities. Finally, binding of  
16 recombinant human FSH to MS-Hu6 in a final formulation (20 mM phosphate buffer, 1 mM NaCl,  
17 0.001% w/v Tween 20, and 260 mM trehalose) resulted in a thermal shift (increase in  $T_m$ ) for the  
18 Fab, but expectedly not in the Fc domain. Given that we used a low dose of MS-Hu6 (1  $\mu$ M), the  
19 next challenge would be to determine whether 100-fold higher, industry-standard concentrations  
20 are equally stable.

21

## 1 **INTRODUCTION**

2           With the approval of the first monoclonal antibody in 1986, the landscape of  
3 immunoglobulins as biotherapeutics has undergone transformation [1]. However, the  
4 development for therapeutic antibodies is complex, due mainly to protein–protein interactions that  
5 lead to antibody aggregation, degradation, deamidation, reduction, oxidation, or interactions  
6 between different domains, such as Fab–Fc or Fab–Fab interactions [2]. Aggregated or degraded  
7 antibodies can also become immunogenic due to the exposure of ‘foreign’ epitopes. Given that  
8 most therapeutic antibodies are injected intravenously or subcutaneously, and require  
9 concentrations >100 mg/mL, human use requires antibodies to be formulated in a way that they  
10 remain stable over time [3].

11           A typical therapeutic antibody is formulated at an acidic pH with salts, sugars, and  
12 stabilizers—each of which serve distinct and overlapping functions in ensuring stability [4]. Most  
13 antibodies display reduced solubility and increased precipitation at the isoelectric pH (pI) [2, 5],  
14 and must therefore be formulated at a pH away from their pI. With highly concentrated antibodies,  
15 the use of inorganic salts improves colloidal stability by shielding free residues from self–  
16 interaction and precipitation. Salts also maintain isotonicity, which is of particular importance in  
17 preventing pain at the injection site. However, higher salt concentrations can lead to precipitation  
18 or “salting” out [6] . Sugars likewise contribute to isotonicity [7], and by being preferentially  
19 excluded from antibody surfaces, improve stability. However, sugars can also cause antibody  
20 glycation, which, in turn, affects half–life. Most therapeutic antibodies thus use non–reducing  
21 sugars. Finally, while detergents and stabilizers can cause antibody degradation, very low  
22 concentrations protect against degradation caused by agitation and sheer stress that often results  
23 from antibody adsorption onto air–solution interfaces [2] .

1           Based on our studies that have established a causal role for the pituitary hormone, follicle-  
2 stimulating hormone (FSH), in regulating bone mass, body composition and neuronal function,  
3 we have created a first-in-class humanized antibody that, we find, reduces body fat, induces  
4 thermogenic adipose tissue and increases bone density [8-14]. The antibody, *hitherto* termed  
5 MS-Hu6, was humanized from a parent monoclonal antibody, Hf2, that was raised against a short,  
6 13-amino-acid-long receptor-binding sequence of FSH $\beta$  [9]. By binding to FSH $\beta$ , MS-Hu6  
7 blocks its interaction with the FSH receptor (FSHR) with high affinity ( $K_D \sim 7.5$  nM) that approaches  
8 that of trastuzumab ( $K_D \sim 5$  nM, Herceptin<sup>®</sup>) [8]. Using a protein thermal shift assay (also termed  
9 differential scanning fluorimetry), we have previously confirmed the stability of MS-Hu6 and its  
10 binding to FSH.

11           Here, we describe detailed steps to develop a formulation with maximal stability and ligand  
12 binding. To do so, we used the protein thermal shift assay to test 217 formulations combining  
13 salts, sugars, and stabilizers at different pH values to derive a near-final formulation ensuring  
14 maximal stability. The formulation was developed and optimized using Food and Drug  
15 Administration (FDA)-approved excipients at concentrations that fall within the inactive ingredient  
16 guide limits for excipients. The protocols, methodologies and analytical evaluations were  
17 developed, recorded, and archived within MediaLab using our Good Laboratory Practices-  
18 complaint platform.

19

## 20 **MATERIALS AND METHODS**

### 21 **Protein Thermal Shift Assay**

22           The protein thermal shift assay, a tool for testing protein unfolding in real-time, is utilized  
23 routinely to screen conditions for maximum protein stability, determine protein-ligand interactions,  
24 and understand protein structure. The fluorescent dye SYPRO-orange is added to the protein

1 solution, which is exposed to incremental increases in temperature ranging from 25 to 99°C.  
2 Protein unfolding exposes hydrophobic surfaces that interact with SYPRO–orange to yield a  
3 fluorescence signal at 570 nm. The second–degree derivative is used to determine the melting  
4 temperature  $T_m$ —a higher  $T_m$  indicates greater protein stability. When proteins, such as MS-Hu6,  
5 bind ligand, a higher  $T_m$  is required for protein unfolding, resulting in a ‘thermal shift’ derived as a  
6  $\Delta T_m$ .

7 Experiments were thus performed using optically clear 0.1 mL PCR tubes (TempAssure,  
8 # 1402-2300). MS-Hu6 was diluted into 20  $\mu$ L reactions containing buffer and/or excipient of  
9 interest, and 10X SYPRO–orange and sterile water or formulation buffer (respective buffers). MS-  
10 Hu6 in water or phosphate buffer at pH 6.2 were used as controls for baseline thermal stability  
11 ( $N=6$  or 8, respectively). The run conditions in the thermocycler (StepOne Plus, Applied  
12 Biosystems) were: 25 °C for 2 minutes, then to 95 °C, with temperature increments of 0.3 °C every  
13 15 s. Fluorescence intensity was measured at each temperature. Each condition was run in  
14 duplicate ( $n=2$ ). The  $\Delta T_m$  was calculated based on the inflection point of the protein thermal shift  
15 melting curve, and the thermal shift was calculated using the following equation (1),

$$\Delta T_m = T_{mA} - T_{mB} \dots \dots \dots (1)$$

18 **Optimizing Antibody Concentration**

19 MS-Hu6 (IgG1 isotype) was obtained from Genscript (Lot# DD1912741) as liquid  
20 formulation in phosphate–buffered saline (PBS) at a concentration of either 5.17 or 19.06 mg/mL.  
21 ~2 mg was buffer exchanged with sterile cell culture grade water (Corning, Cat # 25-055-CV)  
22 using ultra–centrifugal filtration units (Amicon, # UFC903024; MWCO, 30,000 kDa) equilibrated  
23 with water. MS-Hu6 was concentrated to 500  $\mu$ L and re–diluted with water—this process was  
24 repeated 5 times. The final antibody concentration in water was 4.34 mg/mL (~400  $\mu$ L) as  
25 measured on Nanodrop (OD 280 nm). To optimize the concentration for use in the protein thermal

1 shift assay, MS-Hu6 was diluted into a 10  $\mu\text{M}$  working stock solution, which was diluted serially  
2 (1:3) into 20  $\mu\text{L}$  reaction tubes containing buffer and dye to yield the following concentrations: 10,  
3 3.3, 1.08, 0.359, 0.119, 0.039, 0.013 and 0.004  $\mu\text{M}$ . Assay in triplicates yielded a final optimal  
4 concentration of 1  $\mu\text{M}$  for our studies, although concentrations as low as 4 nM could be detected.

5

## 6 **Buffer and Excipient Preparation**

7 For phosphate, citrate, acetate and histidine buffers, 1 M weak acid/base for each was  
8 prepared and mixed in different proportions to give 0.2 M (for phosphate), 0.1 M (for acetate and  
9 citrate) or 0.05 M (for histidine) working concentrations at various pH levels (Supplementary Table  
10 1). For detergents, a 10% (v/v) stock was prepared for each buffer. For sugars, 1 M stocks were  
11 prepared, sterile-filtered, and diluted into 20  $\mu\text{L}$  final reaction volumes.

12

## 13 **Data Analysis**

14 At each temperature  $T$ , the first derivative ( $\Delta\text{RFU}/\Delta T$ ) was calculated to obtain the rate of  
15 change of fluorescence. To generate smooth melting curves, a rolling average of 10 such values  
16 were plotted against temperature. Peaks, annotated as  $T_m$  and calculated from the slope of the  
17 melting curve (i.e., second derivative), were plotted against pH for each condition.

18

## 19 **Molecular Dynamics Simulations**

20 The models of MS-Hu6 were generated based on human IgG template (PDB id: 1GFV  
21 and 3AUV) using a protocol described in detail by Gera et al [8]. For the molecular dynamics  
22 (MD) simulations, two systems were prepared at 1 mM and 100 mM NaCl, each following the  
23 same protocol. The side chains of the protein were protonated using the protein-prepare  
24 implemented in the high-throughput molecular dynamics (HTMD) suite [15]. This was followed  
25 by the parameterization of the protein using the Amber ff14SB force field [16]. The systems were

1 then solvated using a TIP3P water box, with edges extending to 10 Å from the solute. Each  
2 system was then equilibrated for 5 ns in an NPT ensemble, where the protein backbone was  
3 frozen and the solvent with counter ions were allowed to move. This was followed by an  
4 unrestrained production run of 1000 ns in NVE ensemble at 300 K using the ACEMD MD engine  
5 [17]. The time step was kept at 4fs; periodic boundary condition was utilized and the accuracy of  
6 the particle mesh Ewald was increased, while direct sum tolerance was reduced by an order of  
7 magnitude (0.000001). The root mean–square deviation (RMSD), radial distribution function  
8 analysis was carried out using gromacs analysis tools. The electrostatic surface charge on the  
9 protein was calculated on the final snapshot of the simulation using Adaptive Poisson Boltzmann  
10 Solver [18] implemented in PyMol [19].

11

## 12 **Size Exclusion Chromatography (SEC)**

13 Size exclusion chromatography (SEC) was performed to detect monomer loss using an  
14 AKTA Pure Fast Performance Liquid Chromatography system (Cytiva, Marlborough, MA, USA).  
15 Prepacked SEC columns (Superdex 200 10/300 GL 1×30 cm, particle diameter 13 µm) with  
16 TSKgel guard column SwXL (6 mm× 40 mm) were used for the analysis. SEC was used to  
17 separate the native monomeric proteins from any soluble aggregates in the antibody formulations.  
18 Immediately before the analysis, all samples were diluted to 1 mg/ml using the formulation buffer,  
19 loaded onto the SEC column (500 µl), and eluted isocratically at a flow rate of 0.4 ml/min. The  
20 mobile phase consists of 20 mM phosphate buffer at pH 6.2, 260 mM sucrose, 0.001% w/v Tween  
21 20, and 1 mM NaCl at 25°C. The protein concentration was measured by absorbance at 280 nm.  
22 The area under curve of absorption peaks in the chromatogram was used to determine the %  
23 monomer loss in the antibody formulations. Representative chromatographs were reported.

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## 1 **Dynamic Light Scattering (DLS)**

2 Dynamic light scattering (DLS) was performed to determine the size (hydrodynamic  
3 radius,  $r_h$ ) and homogeneity (polydispersity index, PDI) of the antibody; this provides a readout  
4 for the colloidal stability of the antibody in various formulations. Briefly, 20  $\mu$ l of the MS-Hu6  
5 formulation was diluted into 1 ml using the formulation buffer in a 1 ml disposable micro cuvette  
6 (Malvern Cat. ZEN0040). Using the Zetasizer Nano-ZS 90 system (Malvern Instruments Ltd.,  
7 Malvern, PA, USA), the diluted sample was analyzed on a fixed scattering angle ( $90^\circ$ ) at  $4^\circ\text{C}$  for  
8 60 s. The refractive index of the medium was set at 1.33 and the dynamic viscosities of the  
9 samples were measured for each sample. The data were collected and reported as the Z-average  
10 of the hydrodynamic radius and representative DLS graphs were reported.

11

## 12 **RESULTS**

13 To determine the buffer and pH for stable solution of MS-Hu6, four different buffers with a  
14 pH range from 3 to 8 were screened using protein thermal shift assay. These buffers included 20  
15 mM citrate (pH 2.9 to 6.1), 20 mM acetate (pH 3.6 to 5.6), 20 mM phosphate (pH 5.6 to 8.0) and  
16 25 mM histidine (pH 5.0 to 7.0) as shown in (Supplementary Table 1). IgG unfolds with increasing  
17 temperature with two peaks corresponding to unfolding of Fc and Fab regions. Figure 1A shows  
18 representative thermal traces of the Fc and Fab peaks in the four buffers, with each at two pHs  
19 within the aforementioned ranges. Figure 1B displays cumulative data on change in  $T_m$  with  
20 increasing pH in different buffers. Both Fab and Fc regions were relatively stable between pH 5.5  
21 and 6.5, with  $T_m$  dropping precipitously at lower pH values (Figure 1B). Maximum stability was  
22 attained at pH 5.62 for Fab in phosphate buffer, and at pH 6.85 for Fc in histidine buffer (Figure  
23 1C). We therefore focused on further developing phosphate and histidine buffers.

24 We screened for concentration effects to find no difference between 10, 20 and 40 mM  
25 phosphate for the Fab fragment (Figure 1D). However, for the Fc fragment, 10 mM phosphate



1 showed better stability, although at pH 6.2 all three concentrations had similar  $T_m$ s. Given that  
2 our main aim was to optimize the stability of Fab domain, the next set of experiments used 20  
3 mM phosphate buffer at pH 6.2. This was therefore tested in multiple runs within the 5.6 to 7.0  
4 pH range. Average  $T_m$ s for Fab and Fc for Formulations 51–58 are shown in Table S2. Maximum  
5 stability was obtained at pH 5.76 ( $T_m = 79.96 \pm 0.13$ ) for Fab and pH 7.01 ( $T_m = 71.12 \pm 0.36$ ) for  
6 Fc.

7 Salts reduce viscosity, allow stable ionic interactions, increase solubility, and provide  
8 isotonicity. Whether salts stabilize or aggregate a protein depends on its structure and type of  
9 interactions [20, 21]. We used isotonic NaCl (150 mM) without (Formulations 67–73) or with 5  
10 mM KCl (Formulations 74–81) (Table S3). For the Fab domain,  $T_m$  was 79.3°C (pH 6.09),  
11 whereas for the Fc domain, it was 70.9°C (pH 6.78) (Figure 1E and Table S3). Addition of KCl  
12 led to no change or a reduction in  $T_m$ s for Fab (79.03°C at pH 5.76) and Fc (70.58°C at pH 6.8),  
13 respectively. Fab was most stable with phosphate buffer without salt, at a pH of 5.76 for Fab and  
14 7.01 for Fc (Figure 1E). Thus, the presence of KCl had a negative effect on antibody stability,  
15 with a reduction in  $T_m$  by  $\sim 1^\circ\text{C}$ . This is because, it could increase the hydrophobic interactions,  
16 thus destabilizing and denaturing antibodies [20, 22, 23].

17 Stabilizers are required to maintain colloidal stability of monoclonal antibodies; their effect  
18 depends upon the type and concentration of the stabilizer. During stabilizer optimization, two  
19 critical parameters are considered—antibody aggregation and detrimental structure perturbation.  
20 We tested the effect of three stabilizers, namely Tween 20 and Tween 80, and Poloxamer 188,  
21 a copolymer of polyoxypropylene and polyoxyethylene. The two former molecules have been  
22 used traditionally to improve antibody solubility [24–27]. All stabilizers were first screened at  
23 0.001% (w/v) in the presence of 150 mM NaCl and 5 mM KCl (Figure 2A and 2B). For Tween 20,  
24 the Fab region displayed a  $T_m$  of 79.21 °C (pH 6.2), whereas Fc showed a  $T_m$  of 70.32 °C (pH  
25 7.01) (Formulations 82–89, Table S4). For Tween 80, the  $T_m$  for the Fab region was lower at

1 78.93 °C (pH 5.99) (Formulations 90–97, Table S5), while the Fc region melted at 70.58 °C (pH  
2 7.01). For poloxamer 188 (Formulations 98–105, Table S4),  $T_{ms}$  for Fab and Fc were 78.8°C (pH  
3 5.99) and 70.43 (pH 6.62), respectively. This showed that, while the addition of KCl reduced  $T_m$   
4 by 0.5 °C (Figure 1E), this reduction was reversed by the addition of Tween 20. Moreover, high  
5 stabilizer concentration, which leads to strong binding, could destroy and destabilize antibody  
6 structure [27].

7 MS-Hu6 stability was also tested in combinatorically with the following—150, 100, 50 or 1  
8 mM NaCl plus 0.001% w/v Tween 20 in 20 mM phosphate buffer (Figure 3A and 3B). At 150 mM  
9 NaCl (Formulations 114–121, Table S5), the highest  $T_{ms}$  for Fab and Fc were at pH 5.99  
10 (78.78°C) and 6.8 (70.51°C), respectively. At 100 mM NaCl (Formulations 122–129, Table S5)  
11  $T_{ms}$  for Fab and Fc increased to 79.25°C (pH 6.42) and 70.88°C (pH 7.01), respectively. At a still  
12 lower NaCl concentration of 50 mM NaCl, the  $T_m$  further increased to 79.57°C (pH 5.99) for Fab  
13 and 71.04°C (pH 6.81) for Fc. At a 50-fold lower concentration of NaCl (1 mM),  $T_m$  for Fab was  
14 80.2°C (pH 5.99) and that for Fc was 71.15°C (pH 6.81). Overall, therefore, as the salt  
15 concentration decreased the  $T_m$  (stability) increased by ~0.3 to 0.5°C as shown in Figure 3B.

16 Monoclonal antibodies are generally more soluble in dilute salt solutions, as salts in their  
17 ionic forms are attracted towards opposite charges within the antibody moiety, which enhances  
18 surface hydration. However, very high salt concentrations increase water surface tension, and in  
19 doing so, trigger competition between the antibody and salt ions for hydration. Salts strip the vital  
20 layers of water molecules from the protein surface, resulting in a decrease in the intermolecular  
21 hydrogen bonds, antibody solubility and ligand antibody binding, as well as an increase in  
22 hydrophobic interactions; the latter destabilizes and denatures the antibody. This could be the  
23 reason for the noted decrease in  $T_{ms}$  for antibodies at higher salt concentrations [20, 22, 23].

1 To rationalize the effect of salt concentration on the stability of the MS-Hu6, MD  
2 simulations were performed under two ionic conditions of 1 mM and 100 mM NaCl. MD  
3 simulations have been used to investigate the conformational changes under the influence of ionic  
4 salt concentration [28, 29]. The C $\alpha$ -RMSD was used to check the stability of MS-Hu6. The C $\alpha$ -  
5 RMSDs were comparable and minor differences between the two systems at both salt  
6 concentrations. The C $\alpha$ -RMSD of the two chains are illustrated in Figure 3C. Overall, MS-Hu6  
7 in 1 mM displayed higher stability than in 100 mM NaCl. Next, the localization of the ions relative  
8 to the protein surface was assessed using the radial distribution function (RDF). The minimal  
9 distance between the ions and the protein were calculated as a variation of time. The distance  
10 varies from a contact distance of  $\sim 2$  Å and was cutoff at 5 Å. In the simulations with 1 mM NaCl,  
11 the minimal distances between the ions and protein was greater than that observed under 100  
12 mM (Figure 3D). The RDF analysis indicates that the ions are located closer to the protein surface  
13 within the cutoff distance, in accordance with the higher concentration of ions in the solution. The  
14 charged ions localized around the protein surface have the ability to influence side chain  
15 interactions and alter the electrostatic surface charge pattern of the complex (Figure 3E). This  
16 will, in turn, influence protein–protein interactions and possible binding affinities.

17 Polysaccharides and their derivatives minimize the aggregation of antibody during stress  
18 [30]. To determine whether the addition of a sugar enhanced the stability of MS-Hu6, we tested  
19 the above formulation (1 mM NaCl, 0.001% w/v Tween 20 and 20 mM phosphate) with sucrose,  
20 dextran 40, trehalose, sorbitol, or mannitol (260 mM) (Figure 4). With the addition of 260 mM  
21 sucrose (Formulations 146–153, Table S6), the highest  $T_m$ s for Fab and Fc were 80.84°C (pH  
22 5.76) and 72.39°C (pH 6.6), respectively. Of note is that we achieved the highest  $T_m$  for Fab with  
23 the addition of 260 mM trehalose (Formulations 170–177, Table S6) at 81.67°C (pH 6.2), while  
24 for Fc, the  $T_m$  also improved to 73.29°C (pH 6.8). Overall, when compared against 20 mM  
25 phosphate buffer alone, the presence of nonreducing disaccharides led to stabilization of both

1 Fab and Fc region by  $\sim 2$  °C. It is known that polyols and sugars can stabilize an antibody's native  
2 structure by increasing the free energy of unfolding, which thermodynamically favors the natively  
3 folded states of antibodies [30-32].

4 The alcoholic sugars, namely, sorbitol and mannitol (260 mM each), displayed slightly  
5 different characteristics. In the presence of 260 mM sorbitol (Formulations 202–209, Table S6)  
6 the maximum stability of Fab was 80.15°C (pH 5.76). For Fc, the highest  $T_m$  was 72.35°C (pH  
7 6.81). For mannitol (Formulations 210–217, Table S6), the  $T_m$  for Fab and Fc were 80.77°C (pH  
8 5.6) and 71.72°C (pH 6.62), respectively. These alcoholic sugars thus gave very similar  $T_m$ s to  
9 those observed with just 20 mM phosphate buffer, and better  $T_m$ s than those noted with salts.  
10 Formulations containing 260 mM dextran 40 were also screened for thermal stability  
11 (Formulations 194–201, Table S7). At pH 5.76, it showed maximum stability of Fab at 80.17°C  
12 and for Fc at 71.03°C (pH 6.8). In all, a comparison of  $T_m$ s at pH 6.2 (Figures 4A and 4B) showed  
13 that maximum stability was with trehalose, followed by sucrose, sorbitol, mannitol and finally  
14 dextran 40. From these experiments it could be surmised that trehalose improved the stability of  
15 both Fab and Fc domains to the highest  $T_m$ .

16 We next added sucrose and NaCl in different concentrations such that total osmolality  
17 remained constant (Figure 4E and F). The addition of 200 mM sucrose and 50 mM NaCl with 20  
18 mM phosphate and 0.001% w/v Tween 20 (Formulations 154–161, Table S7) resulted in a highest  
19  $T_m$  of 80.18°C (pH 5.8) for Fab, with a lower  $T_m$  of 71.65°C (pH 7.01) for Fc. Furthermore,  
20 changing the sucrose and NaCl concentrations to 100 mM for each led to shifts in thermal stability.  
21 For Fab, the highest  $T_m$  noted was 79.54°C (pH 5.99), and for Fc was 71.57°C (pH 6.81). This  
22 indicated that increasing salt and decreasing sugar concentration reduced thermal stability by  
23  $\sim 0.7$ °C for Fab, with minimal effects on Fc (Figure 4E and 4F). However, the  $T_m$ s of antibody  
24 determined with 260 mM sucrose were still higher at 80.8 ( $\sim 0.5$ °C higher) for Fab and 72.44°C  
25 ( $\sim 0.8$ °C) for Fc.

1 A similar pattern was seen in trehalose (Figure 4C and 4D). The addition of 200 mM  
2 trehalose and 50 mM NaCl (Formulations 178–185, Table S7) resulted in the highest  $T_m$  of  
3 80.42°C (pH 5.99) for Fab and 71.96°C (pH 6.81) for Fc. On decreasing trehalose concentration  
4 to 100 mM and increasing NaCl to 100 mM (Formulations 186–193, Table S7), the highest  $T_m$  for  
5 Fab and Fc both decreased slightly to 79.85°C (pH 5.76) and 70.93 °C (pH 6.62), respectively.  
6 Thus, while decreasing trehalose led to slight decline in  $T_m$ s for Fab and Fc (Figure 4C and 4D),  
7 260 mM trehalose gave maximum stability at 81.67°C for Fab and 72.88°C for Fc. Thus, once  
8 again, the presence of increasing amounts of salts led to a decrease in thermal stability.

9 This trend was again reflected at pH 6.2. Highest  $T_m$ s for Fab were noted for Formulation  
10 181 that contained 200 mM trehalose followed by Formulation 157 that contained 200 mM  
11 sucrose. The next most stable condition was Formulation 189 containing 100 mM trehalose  
12 followed by Formulation 125 containing 100 mM NaCl. This was followed by Formulation 133  
13 containing 50 mM NaCl, and Formulation 165 that contained 100 mM sucrose and 100 mM NaCl.  
14 Finally, while screening across different pHs, salts, sugars, and detergents, as well as optimizing  
15 their concentrations, we found that the best condition configured was a pH 6.2 formulation in 20  
16 mM phosphate, 260 mM trehalose, 1 mM NaCl and 0.001% w/v Tween20 (Formulation 173, Table  
17 S6) as shown in Figure 4.

18 After confirming the conditions for optimal stability of MS-Hu6, we tested its binding to  
19 FSH. For this set of experiments, 1  $\mu$ M MS-Hu6 was incubated with 10  $\mu$ M of FSH and its thermal  
20 stability was measured. This was performed in the following conditions: 20 mM phosphate at four  
21 different pH levels (5.76, 5.99, 6.20 and 6.42), plus, for each condition, 0.001% w/v Tween20 and  
22 1 mM NaCl. Binding was tested in 260 mM trehalose and 260 mM sucrose in the presence or  
23 absence of FSH.  $\Delta T_m$  was calculated from the changes measured within each condition (Figure  
24 5A). At pH 6.2, in case of phosphate buffer,  $\Delta T_m$  for Fab was 3.07°C. On addition of excipients  
25 with 260 mM trehalose (Figure 5B), the  $\Delta T_m$  for Fab was 3.01°C. In the presence of 260 mM

1 sucrose, the  $\Delta T_m$  was 2.68°C (Figure 5C). Thus, the presence of FSH led to a shift in  $T_m$  to the  
2 right for Fab by ~2.5 to 3°C (Figure 5A–C). Notably, and as a control, Fc remained relatively  
3 unchanged (~0.5°C to the left). In the presence of trehalose at pH 6.2,  $\Delta T_m$  on addition of FSH  
4 was ~3°C higher irrespective of whether it was with phosphate or histidine (Figure 5B). Likewise,  
5 in the presence of sucrose,  $\Delta T_m$  was ~2.7°C (Figure 5C).

6 Using SEC, MS-Hu6 in this optimized formulation and in PBS were evaluated for  
7 aggregation (formation of high molecular weight species, HMS) and fragmentation (formation of  
8 low molecular weight species, LMS). MS-Hu6 in the optimized formulation retained a slightly  
9 higher fraction of monomers (99.41%, Peak 2) compared with MS-Hu6 in PBS (99.27%) (Figure  
10 6A). The % monomer loss in either buffer was <1%, indicating that there was minimal  
11 fragmentation or aggregation, and is within the acceptable limit (5–10%).

12 Furthermore, formulation (1 mg/ml) and MS-Hu6 standard (1 mg/ml) were tested to  
13 confirm the heterogeneity and aggregation at the nano level using DLS. This study recorded size  
14 in terms of hydrodynamic radius and PDI as indicators of aggregation and heterogeneity. The  
15 DLS data of the MS-Hu6 (in PBS) were found to be polydisperse in nature, with a PDI value of  
16 0.74 (Figure 6B). And the hydrodynamic radius of the major volume (99.07%) was found to be  
17 4.50 nm (Figure 6B). The MS-Hu6 sample could contain 0.3 % soluble subvisible aggregated  
18 particles with a hydrodynamic radius of 96.04 nm (0.1% volume) and 2789 nm (0.20 % volume),  
19 respectively. However, in the case of formulated MS-Hu6, PDI was reduced and found to be 0.41  
20 (Figure 6B). The hydrodynamic radius of the major volume (99.90 %) was found to be 4.05 nm  
21 (Figure 6B), suggesting the reduction of size and PDI compared to unformulated antibodies. The  
22 soluble subvisible aggregated particles in formulated antibodies were found to be decreased to  
23 0.1% volume as compared to unformulated samples. That was not even detectable due to the  
24 minimal volume. In the formulation, these aggregated particles could be dissolved or solubilized  
25 in the presence of a stabilizer and other excipients and could maintain colloidal stability.

## 1 **DISCUSSION**

2           In this study we determined the thermal stability of an FSH–blocking antibody MS-Hu6  
3 using thermal shift assay to estimate  $T_{ms}$  in 217 different formulations consisting of combinations  
4 of pH, salts, sugars and detergents/stabilizer using our GLP–compliant platform. Beginning by  
5 determining the pH range within which the Fab and Fc showed stability, we noted that these two  
6 regions behaved distinctly [7]. Phosphate buffer provided higher stability to the Fab region,  
7 whereas histidine buffer improved Fc stability. The Fab region seemed to be stable at a pH of  
8 5.6, whereas Fc had improved stability at a pH of 6.9. In contrast, concentration of buffer ions  
9 impacted the behavior of Fc region, but did not appreciably alter the Fab region.

10           The Fab region of an IgG molecule contains the antigen binding domain, and the structural  
11 conformation and stability of this region is paramount when targeting a ligand for inhibition. The  
12 Fc region is also important in that it ensures a longer half–life and optimal pharmacokinetics for a  
13 therapeutic antibody. Therefore, in our studies, while we selectively focused on conditions that  
14 would give maximum stability to the Fab region, we also ensured the Fc region was within an  
15 acceptable range of stability. In addition, we ensured that the pH of the formulation would be as  
16 further away as possible from the isoelectric point, where the solubility would be minimal and the  
17 tendency for aggregation would increase. With this in mind, we screened for the stability of the  
18 Fab and Fc regions in the range of pHs between 5.6 to 7.0, with excipients added, while also  
19 concentrating on pH 6.2 (determined to be optimal pH for Fab in some conditions) [33].

20           We tested excipients that are most prevalent in marketed therapeutic antibody  
21 formulations [34, 35]. Around 50% of commercial formulations tend to have NaCl [35, 36]. Thus,  
22 we first screened NaCl and KCl, at concentrations that closely matched physiology. Interestingly,  
23 we saw a decline in the stability of both Fab and Fc regions, especially in the lower pH range (for  
24 the Fc region). Particularly at pH 6.2, we noted both Fab and Fc stability decline by 0.8 °C upon

1 the addition of salt, suggesting that salts reduce stability. Next, we screened detergents  
2 (stabilizers) as vital for preventing antibody degradation with agitation stress. To determine if the  
3 presence of detergents/stabilizers would improve thermal stability after the decline with salts, we  
4 tested three stabilizers in the presence of salts. We noted that Fab was more stable upon the  
5 addition of 0.001 % w/v Tween 20, whereas Tween 80 performed better for Fc stability. However,  
6 20 mM phosphate buffer still gave better stability in comparison, and the stabilizers could not  
7 rescue the salt-induced decline in thermal stability.

8 Concluding that the presence of salts seemed to have a destabilizing effect on the  
9 antibody, in the next set of experiments we moved to reduce salts to 1 mM and added 260 mM  
10 sugars with 0.001% w/v stabilizer. Here, we saw a remarkable improvement in melting  
11 temperatures for both Fab and Fc. In the presence of each sugar, we saw a rise in  $T_m$ s by at  
12 least 1–2 °C at best, and  $T_m$ s comparable with 20 mM phosphate at worst. Thus, the presence  
13 of sugars benefited the stability of MS-Hu6, potentially through interactions of glycosylated amino  
14 acids with the sugars. We also confirmed the stability of MS-Hu6 in sugar and salt titration  
15 experiments, where increasing amounts of salts and decreasing amounts of sugars were tested,  
16 either combinatorically or separately. Here, we again noted that decreasing salt concentrations  
17 had a marginally positive effect on the  $T_m$ s of Fab and Fc regions. Surprisingly, adding sugars to  
18 salts did not strongly mitigate the negative effect of salts on the Fab region. The best noted  $T_m$   
19 was with 20 mM phosphate buffer at pH 6.2 in the presence of 260 mM trehalose or sucrose, 1  
20 mM NaCl and 0.001% w/v Tween 20—this was deemed as our final low-dose formulation. This  
21 experimental observation was further corroborated using MD simulations, which highlighted  
22 improved stability of MS-Hu6 at low salt concentration, consistent with the reduced localization of  
23 ions around the protein and their ability to influence side chain interactions.

24 Finally, we tested the binding of MS-Hu6 to FSH in the presence of this final formulation  
25 within a narrow pH range. We compared this to alternative formulations consisting of 10 mM



1 histidine (instead of 20 mM phosphate) and sucrose (instead of trehalose). We saw a 3 °C shift  
2 in the Fab region, which is comparable to previous experiments. Importantly, the final formulation  
3 did not seem to impact the ability of MS-Hu6 to interact with its ligand. We did not see major  
4 differences in binding capability between histidine and phosphate buffers, as in both instances, a  
5 shift in stability of Fab through interaction with FSH was evident.

6 Monomer loss in the formulated antibody and MS-Hu6 in PBS, determined in our SEC  
7 study, was less than 1% and within the permissible range of 5-10% observed in commercially  
8 available biopharmaceutical products. Typically, a maximum of 5% monomer loss is the  
9 acceptable threshold [37]. Dimers, which are reversible structures formed from soluble subvisible  
10 particles, contribute to minimum aggregation and are not critical in biopharmaceutical product  
11 development [4]. These particles may diminish in the presence of an efficient stabilizer. However,  
12 antibody fragmentation or multimerization forming insoluble irreversible clumps are critical in the  
13 development of biopharmaceuticals. For this, excipients are used to stabilize the monomeric form  
14 of antibodies at higher concentrations [32]. Any protein formulation must achieve high long-term  
15 stability, which requires maximizing the monomeric fraction and minimizing multimer formation or  
16 fragmentation [37].

17 In the DLS study, no significant aggregation was observed in either sample, which is less  
18 than 1% of the total volume. In both cases, samples maintained the monomeric form with minimal  
19 or no aggregated particles. Because of their reversible nature, these aggregates are impractical  
20 to eliminate below certain levels, so that these subvisible soluble particles are well-accepted by  
21 the US pharmacopeia (USP) and US FDA (5-10%) in the final optimized formulation [38].  
22 Furthermore, they could not affect the colloidal stability and structural integrity of antibody in the  
23 formulation [39]. Most notably, bigger and irreversible particles need to be controlled because  
24 they could precipitate out of solution when protein exceeds the solubility limit. According to FDA  
25 guidelines, these particles are of different sizes; while particles of 150 µm are visible [40], most

1 particle below this sizes could elicit immune reactions [41, 42]. The particles with sizes of  $\leq 50$ -  
2 100  $\mu\text{m}$  are considered to be subvisible particles. However, a size  $\geq 10 \mu\text{m}$  can obstruct or  
3 interfere with blood flow [43]. Chapter 788 of the USP is on the subvisible particle counting  
4 method, which set acceptable limits for particulate matter in a container ( $\leq 100 \text{ ml}$  to be 6000  
5 particles  $\geq 10 \mu\text{m}$  and 600 particles  $\geq 25 \mu\text{m}$ ) [43]. However, because the majority of biological  
6 products are currently administered intravenously or subcutaneously, the FDA has strict  
7 regulatory guidelines in place that take the 10  $\mu\text{m}$  threshold limit of aggregates into account in  
8 order to prevent blood vessel occlusion. Additionally, this might help to maintain long-term  
9 colloidal stability of the biopharmaceutical product [44]. In all, while we have successfully  
10 formulated MS-Hu6 at a low concentration of 1  $\mu\text{M}$ , the next is to determine whether the  
11 formulation will provide equal stability to a 100-fold higher, industry-standard, concentration.  
12 Furthermore, it would be critical to compare if each of the excipients offers protection against  
13 antibody degradation pathways, particularly in response to heating, freeze-thaw cycles, and  
14 agitation.

15

1 **AUTHOR CONTRIBUTIONS**

2 D.S., S.R., S.G., and S.H.: Conceptualization, data curation, formal analysis, validation,  
3 investigation, visualization, methodology, writing—original draft, writing—review and editing.  
4 A.R.P. and T.-C.K.: Data curation, formal analysis, investigation, and visualization. A.P., F.K.,  
5 L.C., J. Chatterjee, E.S., S.M., F.S., and J.G.-R.: Data curation, formal analysis, investigation,  
6 and visualization. O.B. and A.M.: Data management and provenance. C.R.: Conceptualization.  
7 M.M. and J. Caminis: GLP management and methodology. C.J.R.: Conceptualization and  
8 methodology. D.L., V.R., and S.-M.K.: Data curation, formal analysis, investigation, and  
9 methodology. T.Y. and M.Z.: Conceptualization, supervision, writing—original draft, writing—  
10 review and editing.

11  
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19  
20 **COMPETING INTERESTS**

21 M.Z. is an inventor on issued patents on inhibiting FSH for the prevention and treatment  
22 of osteoporosis and obesity (U.S. Patent 8,435,948 and 11,034,761). M.Z. is also an inventor on  
23 a pending patent application on the composition and use of humanized monoclonal anti–FSH  
24 antibodies and is a co-inventor of a pending patent on the use of FSH as a target for preventing

1 Alzheimer's disease. These patents are owned by Icahn School of Medicine at Mount Sinai  
2 (ISMMS), and M.Z. would be recipient of royalties, *per* institutional policy. M.Z. also consults for  
3 several financial platforms, including Gerson Lehman Group and Guidepoint, on drugs for  
4 osteoporosis and genetic bone diseases.

5

## 1 LEGENDS TO FIGURES

2  
3 **Figure 1:** Screening of different buffer conditions and pHs to obtain a stable MS-Hu6 solution.  
4 (A) 20 mM citrate buffer (pH 2.9–6.1), 20 mM acetate buffer (pH 3.6–5.6), 20 mM phosphate  
5 buffer (pH 5.6–8.0), and 25 mM histidine buffer (pH 5.0–7.0). (B) Representation of the  
6 cumulative data on change in  $T_m$  with increasing pH in different buffer conditions. (C) Maximum  
7 stability of the Fab and Fc domains; at pH 5.62 for Fab in phosphate buffer, and at pH 6.85 for Fc  
8 in histidine buffer. (D) Effect of phosphate buffer concentrations (10, 20, and 40 mM) on stability  
9 of the Fab and Fc domains of MS-Hu6. (E) Effect of 20 mM phosphate buffer containing 150 mM  
10 NaCl and 5 mM KCl on the stability of the Fab and Fc domains of MS-Hu6.

11  
12 **Figure 2:** (A) Effect of stabilizers (Tween 20, Tween 80, and poloxamer 188) on the stability of  
13 the Fab and Fc domains of the MS-Hu6 in a buffer containing 20 mM phosphate, 150 mM NaCl,  
14 and 5 mM KCl at pH 5.5–7.0. In this formulation, Tween 20 at 0.001% yielded the highest stability  
15 at pH 6.2 (B).

16  
17 **Figure 3:** (A) Effect of NaCl concentrations (150, 100, 50, and 1 mM) on the stability of the Fab  
18 and Fc domains of the MS-Hu6 in a buffer containing 20 mM phosphate and 0.001% Tween20 at  
19 pH 5.5–7.0. The most stable formulation at pH 6.2 was with 1 mM NaCl (B). (C) Molecular  
20 dynamics simulation of MS-Hu6 at 1 and 100 mM NaCl concentrations. The  $C\alpha$ -RMSDs were  
21 comparable and minor differences were observed between the two systems at both ionic  
22 concentrations. The  $C\alpha$ -RMSDs of the two chains of the MS-Hu6 are colored red and black. (D)  
23 Ion distribution around the protein surface was assessed using the radial distribution function  
24 (RDF). The minimal distance between the ions and the protein was calculated as a variation of  
25 time. RDF analysis for 100 mM salt simulation indicates that the ions are located closer to the  
26 complex surface within the cutoff distance, in accordance with the higher concentration of ions in

1 the solution. (E) The charged ions localized around the protein surface can influence side chain  
2 interactions and alter electrostatic surface charge pattern.

3

4 **Figure 4:** (A) Effect of sugar (260 mM each, sucrose, trehalose, mannitol, dextran 40, and  
5 sorbitol) on the stability of the Fab and Fc domains of MS-Hu6 in a buffer containing 20 mM  
6 phosphate, 1 mM NaCl, and 0.001% w/v Tween 20 at pH 5.5–7.0. The addition of trehalose  
7 yielded the highest stability at pH 6.2 (B). (C) Effect of trehalose and NaCl concentrations on the  
8 stability of the Fab and Fc domains of the MS-Hu6 at pH 5.5–7.0. Trehalose at 260 mM combined  
9 with NaCl at 1 mM yielded a formulation that is most stable at pH 6.2 (D). (E) Effect of sucrose  
10 and NaCl concentrations on the stability of the Fab and Fc domains of the MS-Hu6 at pH 5.5–7.0.  
11 Similar to trehalose, sucrose at 260 mM combined with NaCl at 1 mM yielded the most stable  
12 formulation at pH 6.2 (F).

13

14 **Figure 5:** Effect of FSH binding to MS-Hu6 on the stability of Fab and Fc domains of MS-Hu6 in  
15 (A) 20 mM phosphate buffer at pH 5.76–6.42, (B) 20 mM phosphate buffer, 1 mM NaCl, 0.001%  
16 w/v Tween 20, and 260 mM trehalose at pH 5.76–6.42, and (C) 20 mM phosphate buffer, 1 mM  
17 NaCl, 0.001% w/v Tween 20, and 260 mM sucrose with at pH 5.76–6.42.

18

19 **Figure 6:** (A) Representative size exclusion chromatography (SEC) chromatographs of MS-Hu6  
20 in PBS and in formulation (1 mg/ml). (B) Representative particle size volume distribution graphs  
21 obtained from dynamic light scattering (DLS).

22

## 1 REFERENCES

- 2 1. An, Z., *Monoclonal antibodies - a proven and rapidly expanding therapeutic modality for*  
3 *human diseases*. Protein Cell, 2010. **1**(4): p. 319-330.
- 4 2. Wang, W., et al., *Antibody structure, instability, and formulation*. J Pharm Sci, 2007. **96**(1):  
5 p. 1-26.
- 6 3. Wang, S.S., Y.S. Yan, and K. Ho, *US FDA-approved therapeutic antibodies with high-*  
7 *concentration formulation: summaries and perspectives*. Antib Ther, 2021. **4**(4): p. 262-  
8 272.
- 9 4. Whitaker, N., et al., *A Formulation Development Approach to Identify and Select Stable*  
10 *Ultra-High-Concentration Monoclonal Antibody Formulations With Reduced Viscosities*.  
11 J Pharm Sci, 2017. **106**(11): p. 3230-3241.
- 12 5. Zheng, S., et al., *Investigating the Degradation Behaviors of a Therapeutic Monoclonal*  
13 *Antibody Associated with pH and Buffer Species*. AAPS PharmSciTech, 2017. **18**(1): p.  
14 42-48.
- 15 6. Le Basle, Y., et al., *Physicochemical Stability of Monoclonal Antibodies: A Review*. Journal  
16 of Pharmaceutical Sciences, 2020. **109**(1): p. 169-190.
- 17 7. Vermeer, A.W. and W. Norde, *The thermal stability of immunoglobulin: unfolding and*  
18 *aggregation of a multi-domain protein*. Biophys J, 2000. **78**(1): p. 394-404.
- 19 8. Gera, S., et al., *First-in-class humanized FSH blocking antibody targets bone and fat*. Proc  
20 Natl Acad Sci U S A, 2020. **117**(46): p. 28971-28979.
- 21 9. Ji, Y., et al., *Epitope-specific monoclonal antibodies to FSHbeta increase bone mass*. Proc  
22 Natl Acad Sci U S A, 2018. **115**(9): p. 2192-2197.
- 23 10. Liu, P., et al., *Blocking FSH induces thermogenic adipose tissue and reduces body fat*.  
24 Nature, 2017. **546**(7656): p. 107-112.
- 25 11. Sun, L., et al., *FSH directly regulates bone mass*. Cell, 2006. **125**(2): p. 247-60.
- 26 12. Xiong, J., et al., *FSH blockade improves cognition in mice with Alzheimer's disease*.  
27 Nature, 2022. **603**(7901): p. 470-476.
- 28 13. Zhu, L.L., et al., *Blocking antibody to the beta-subunit of FSH prevents bone loss by*  
29 *inhibiting bone resorption and stimulating bone synthesis*. Proc Natl Acad Sci U S A, 2012.  
30 **109**(36): p. 14574-9.
- 31 14. Gera, S., et al., *FSH-blocking therapeutic for osteoporosis*. Elife, 2022. **11**.
- 32 15. Doerr, S., et al., *HTMD: High-Throughput Molecular Dynamics for Molecular Discovery*.  
33 J Chem Theory Comput, 2016. **12**(4): p. 1845-52.
- 34 16. Maier, J.A., et al., *ff14SB: Improving the Accuracy of Protein Side Chain and Backbone*  
35 *Parameters from ff99SB*. J Chem Theory Comput, 2015. **11**(8): p. 3696-713.
- 36 17. Harvey, M.J., G. Giupponi, and G.D. Fabritiis, *ACEMD: Accelerating Biomolecular*  
37 *Dynamics in the Microsecond Time Scale*. J Chem Theory Comput, 2009. **5**(6): p. 1632-9.
- 38 18. Jurrus, E., et al., *Improvements to the APBS biomolecular solvation software suite*. Protein  
39 Sci, 2018. **27**(1): p. 112-128.
- 40 19. Package, I.P.S.; Available from: <http://www.pymol.org/pymol>.
- 41 20. Arosio, P., et al., *On the role of salt type and concentration on the stability behavior of a*  
42 *monoclonal antibody solution*. Biophys Chem, 2012. **168-169**: p. 19-27.
- 43 21. Ahmed, S., et al., *The TGF-beta/Smad4 Signaling Pathway in Pancreatic Carcinogenesis*  
44 *and Its Clinical Significance*. J Clin Med, 2017. **6**(1).

- 1 22. Sinha, R. and S.K. Khare, *Protective role of salt in catalysis and maintaining structure of*  
2 *halophilic proteins against denaturation*. Front Microbiol, 2014. **5**: p. 165.
- 3 23. Formanek, M.S., L. Ma, and Q. Cui, *Effects of temperature and salt concentration on the*  
4 *structural stability of human lymphotactin: insights from molecular simulations*. J Am  
5 Chem Soc, 2006. **128**(29): p. 9506-17.
- 6 24. Agarkhed, M., et al., *Effect of Surfactants on Mechanical, Thermal, and Photostability of*  
7 *a Monoclonal Antibody*. AAPS PharmSciTech, 2018. **19**(1): p. 79-92.
- 8 25. Agarkhed, M., et al., *Effect of polysorbate 80 concentration on thermal and photostability*  
9 *of a monoclonal antibody*. AAPS PharmSciTech, 2013. **14**(1): p. 1-9.
- 10 26. Kerwin, B.A., *Polysorbates 20 and 80 used in the formulation of protein biotherapeutics:*  
11 *Structure and degradation pathways*. Journal of Pharmaceutical Sciences, 2008. **97**(8): p.  
12 2924-2935.
- 13 27. Wang, S.J., et al., *Stabilizing two IgG1 monoclonal antibodies by surfactants: Balance*  
14 *between aggregation prevention and structure perturbation*. European Journal of  
15 Pharmaceutics and Biopharmaceutics, 2017. **114**: p. 263-277.
- 16 28. Ross, G.A., et al., *Biomolecular Simulations under Realistic Macroscopic Salt Conditions*.  
17 J Phys Chem B, 2018. **122**(21): p. 5466-5486.
- 18 29. Formanek, M.S., L. Ma, and Q. Cui, *Effects of temperature and salt concentration on the*  
19 *structural stability of human lymphotactin: Insights from molecular simulations*. Journal  
20 of the American Chemical Society, 2006. **128**(29): p. 9506-9517.
- 21 30. Nicoud, L., et al., *Effect of polyol sugars on the stabilization of monoclonal antibodies*.  
22 Biophys Chem, 2015. **197**: p. 40-6.
- 23 31. Sudrik, C.M., et al., *Understanding the Role of Preferential Exclusion of Sugars and*  
24 *Polyols from Native State IgG1 Monoclonal Antibodies and its Effect on Aggregation and*  
25 *Reversible Self-Association*. Pharmaceutical Research, 2019. **36**(8).
- 26 32. Ohtake, S., Y. Kita, and T. Arakawa, *Interactions of formulation excipients with proteins*  
27 *in solution and in the dried state*. Adv Drug Deliv Rev, 2011. **63**(13): p. 1053-73.
- 28 33. Niedziela-Majka, A., et al., *High-throughput screening of formulations to optimize the*  
29 *thermal stability of a therapeutic monoclonal antibody*. J Biomol Screen, 2015. **20**(4): p.  
30 552-9.
- 31 34. Pandey, L.M., *Physicochemical factors of bioprocessing impact the stability of therapeutic*  
32 *proteins*. Biotechnol Adv, 2022. **55**: p. 107909.
- 33 35. Le Basle, Y., et al., *Physicochemical Stability of Monoclonal Antibodies: A Review*. J  
34 Pharm Sci, 2020. **109**(1): p. 169-190.
- 35 36. Ionova, Y. and L. Wilson, *Biologic excipients: Importance of clinical awareness of inactive*  
36 *ingredients*. PLoS One, 2020. **15**(6): p. e0235076.
- 37 37. *A Standard Protocol for Deriving and Assessment of Stability - Part 2: Aseptic*  
38 *Preparations (Biopharmaceuticals)-Edition 3.National Health Service - Pharmaceutical*  
39 *Quality Assurance Committee;2017*. [https://www.sps.nhs.uk/articles/standard-protocol-](https://www.sps.nhs.uk/articles/standard-protocol-for-deriving-and-assessment-of-stability-part-2-aseptic-preparations-biopharmaceuticals-edition-2-2015-yellow-cover/)  
40 [for-deriving-and-assessment-of-stability-part-2-aseptic-preparations-biopharmaceuticals-](https://www.sps.nhs.uk/articles/standard-protocol-for-deriving-and-assessment-of-stability-part-2-aseptic-preparations-biopharmaceuticals-edition-2-2015-yellow-cover/)  
41 [edition-2-2015-yellow-cover/](https://www.sps.nhs.uk/articles/standard-protocol-for-deriving-and-assessment-of-stability-part-2-aseptic-preparations-biopharmaceuticals-edition-2-2015-yellow-cover/).
- 42 38. Pham, N.B. and W.S. Meng, *Protein aggregation and immunogenicity of biotherapeutics*.  
43 Int J Pharm, 2020. **585**: p. 119523.
- 44 39. Wang, W., et al., *Immunogenicity of protein aggregates-Concerns and realities*.  
45 International Journal of Pharmaceutics, 2012. **431**(1-2): p. 1-11.



- 1 40. US-FDA. *Inspection of Injectable Products for Visible Particulates Guidance for Industry*.  
2 December 2021; Available from: [https://www.fda.gov/regulatory-information/search-fda-](https://www.fda.gov/regulatory-information/search-fda-guidance-documents/inspection-injectable-products-visible-particulates)  
3 [guidance-documents/inspection-injectable-products-visible-particulates](https://www.fda.gov/regulatory-information/search-fda-guidance-documents/inspection-injectable-products-visible-particulates).
- 4 41. US-FDA. *FDA, Guidance for industry: immunogenicity assessment for therapeutic protein*  
5 *products*. August 2014; Available from: [https://www.fda.gov/regulatory-](https://www.fda.gov/regulatory-information/search-fda-guidance-documents/immunogenicity-assessment-therapeutic-protein-products)  
6 [information/search-fda-guidance-documents/immunogenicity-assessment-therapeutic-](https://www.fda.gov/regulatory-information/search-fda-guidance-documents/immunogenicity-assessment-therapeutic-protein-products)  
7 [protein-products](https://www.fda.gov/regulatory-information/search-fda-guidance-documents/immunogenicity-assessment-therapeutic-protein-products).
- 8 42. Ratanji, K.D., et al., *Subvisible Aggregates of Immunogenic Proteins Promote a Th1-Type*  
9 *Response*. *Toxicological Sciences*, 2016. **153**(2): p. 258-270.
- 10 43. USP. *USP<788>. Particulate matter in Injections*. USP July 2012; Available from:  
11 [https://www.uspnf.com/sites/default/files/usp\\_pdf/EN/USPNF/revisions/788\\_particulate](https://www.uspnf.com/sites/default/files/usp_pdf/EN/USPNF/revisions/788_particulate_matter_in_injections.pdf)  
12 [matter\\_in\\_injections.pdf](https://www.uspnf.com/sites/default/files/usp_pdf/EN/USPNF/revisions/788_particulate_matter_in_injections.pdf).
- 13 44. Kijanka, G., et al., *Submicron Size Particles of a Murine Monoclonal Antibody Are More*  
14 *Immunogenic Than Soluble Oligomers or Micron Size Particles Upon Subcutaneous*  
15 *Administration in Mice*. *Journal of Pharmaceutical Sciences*, 2018. **107**(11): p. 2847-2859.  
16  
17